

Modulación de Coherencias Cuánticas Intermoleculares debido a difusión molecular restringida en materiales porosos.

Rodolfo Acosta

Imágenes por RMN (MRI)

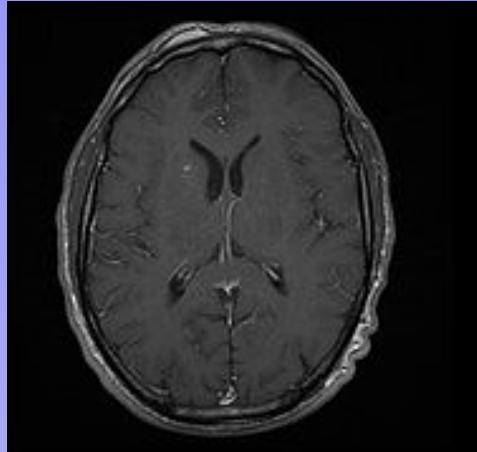


Imagen con secuencia sin contraste

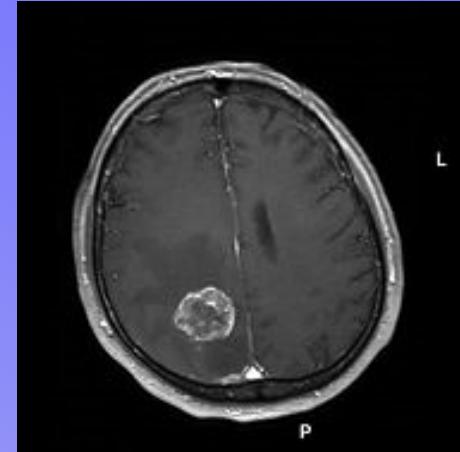
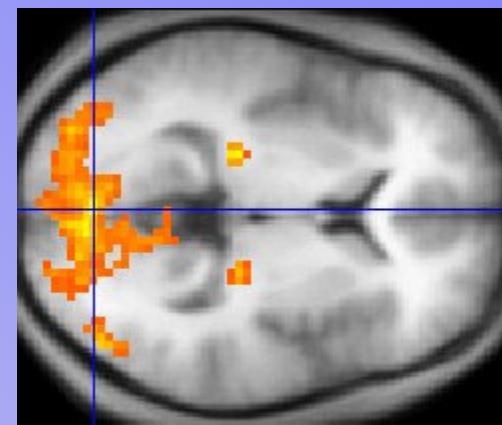


Imagen con contraste de T₁



Imagen con contraste de T₂

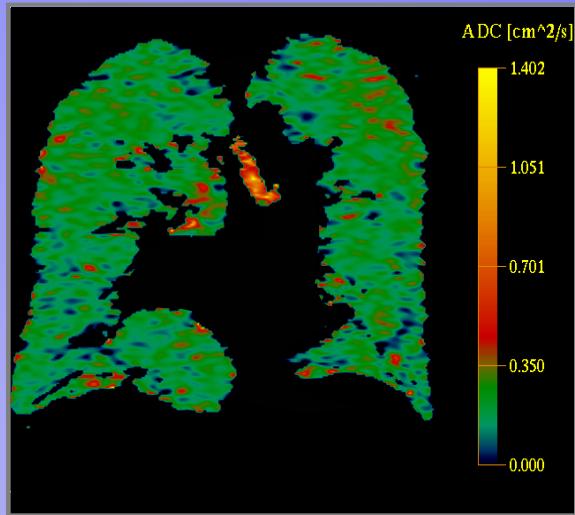


Functional MRI

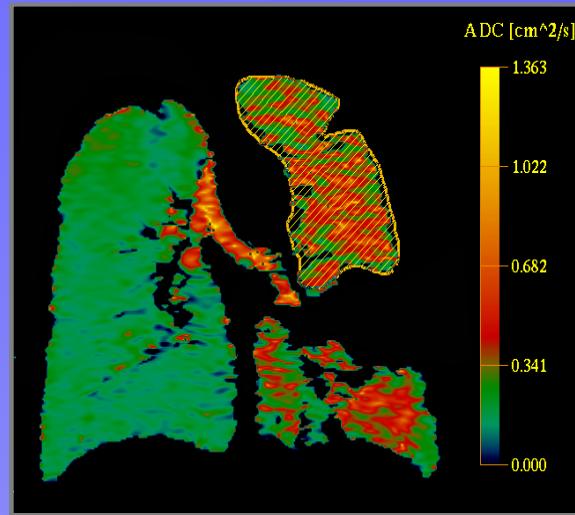
Gas MRI

Imágenes de pulmones con gases hiperoxigenados
 ^3He (^{129}Xe , S^{19}F_6)

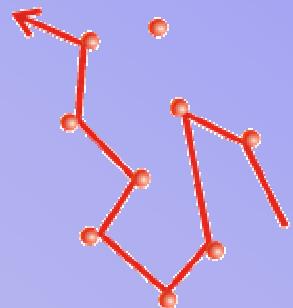




Pulmon sano



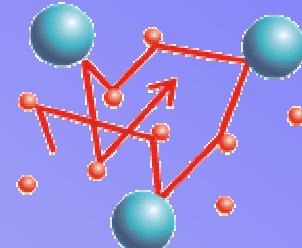
Pulmón con enfisema



Difusión libre



restringida

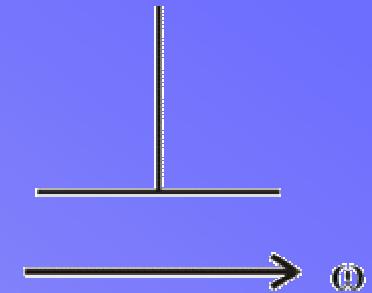
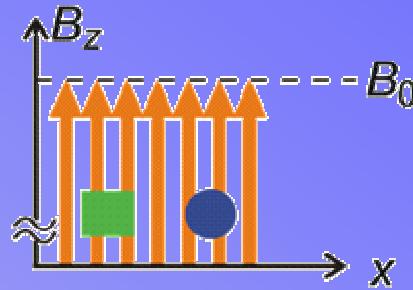
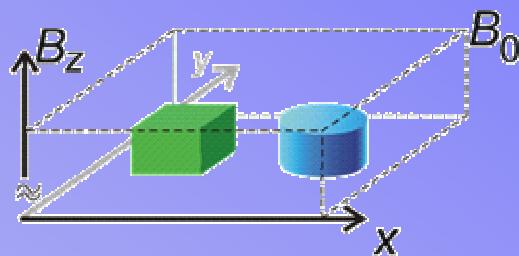


en presencia
de otros gases

RMN – conceptos – Imágenes por RMN

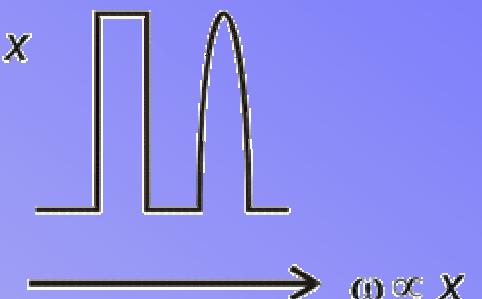
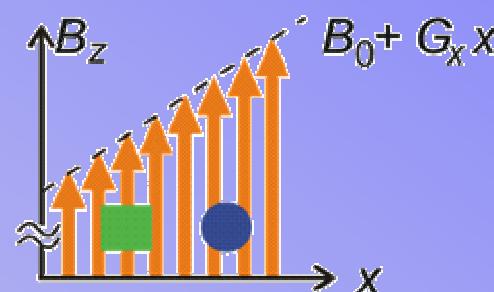
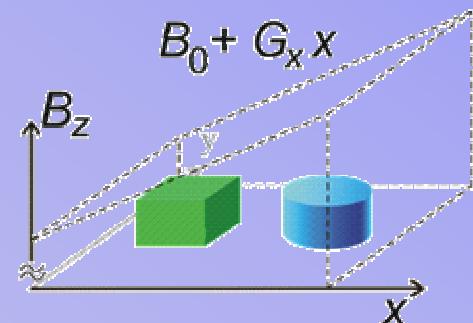
Espectroscopía

$$\omega = \gamma B$$

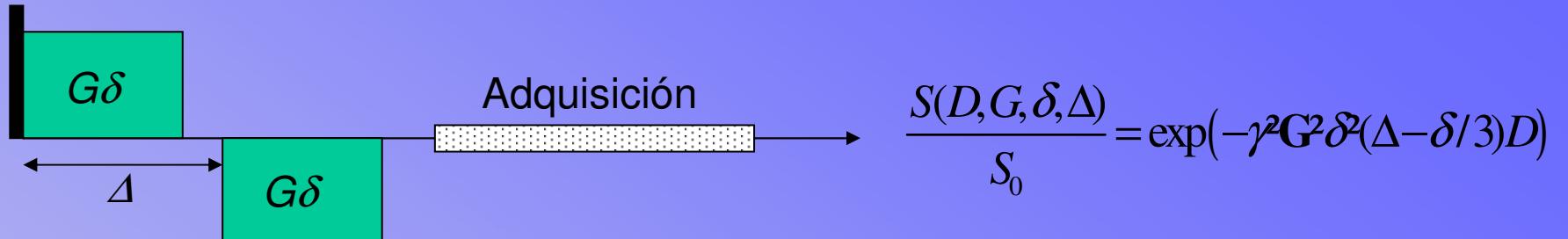


MRI

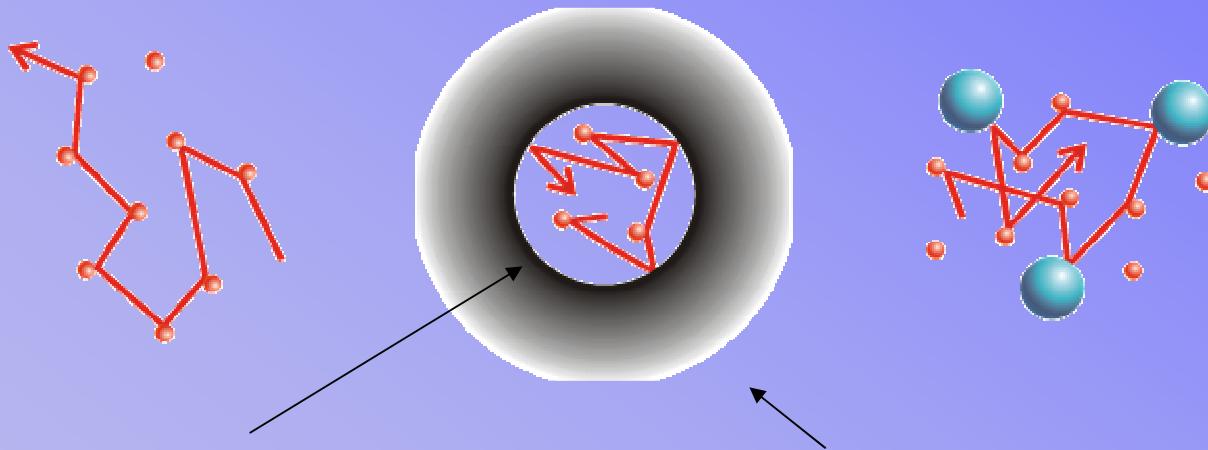
$$G_x = \frac{\partial B_z}{\partial x}$$



Atenuación debido a Difusión



$$\langle [\vec{r}(t) - \vec{r}(0)]^2 \rangle = 2dD(t)t$$



Diferencias de susceptibilidad magnética en las interfases introducen gradientes internos

$D(0)$: medición de tamaño de poro
 $D(t)$: Interconectividad entre poros

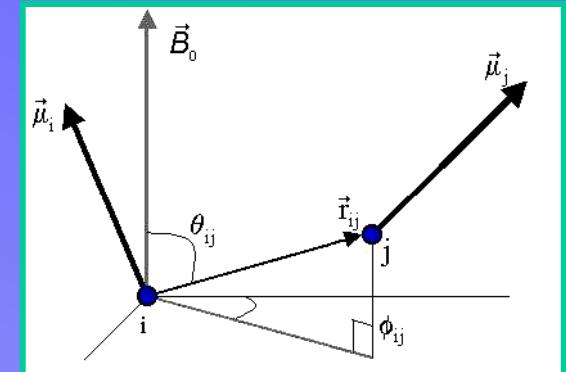
Interacción Dipolar de largo alcance en líquidos

La energía de interacción entre pares de momentos magnéticos

$$H_d = \frac{\mu_i \mu_j}{r_{ij}^3} - \frac{3(\vec{\mu}_i \cdot \vec{r}_{ij})(\vec{\mu}_j \cdot \vec{r}_{ij})}{r_{ij}^5}$$

Hamiltoniano secular

$$H_d^{(0)} = \sum_{i < j} \frac{\mu_0 \gamma^2 \hbar}{4\pi} \frac{1}{r_{ij}^3} \frac{1}{2} (1 - 3 \cos^2 \theta_{ij}) (3I_{iz}I_{jz} - \vec{I}_i \cdot \vec{I}_j)$$



Normalmente se asume que se promedia por movimientos moleculares

SI SE ROMPE LA SIMETRIA EL
PROMEDIO ANGULAR NO SE
CANCELARÁ PARA MOLECULAS
LEJANAS

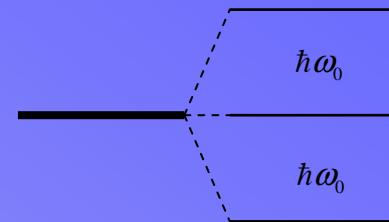
→ Agua T_{amb} difunde 150 μm en 5 seg.

GRADIENTES DE CAMPO ESTATICO

Construcción de la Matriz Densidad en líquidos

Despreciando cualquier interacción salvo Zeeman

$$\rho_{eq} = \frac{\exp(-H/kT)}{\text{Tr}\{\exp(-H/kT)\}} = \frac{\prod_i \exp(-\hbar\omega_0 I_{zi}/kT)}{\text{Tr}\{\exp(-H/kT)\}}$$



Asumiendo distribución Gaussiana

$$\rho_{eq} = 2^{-N} \exp\left(-\sum_i \frac{\hbar\omega_0}{kT} I_{zi}\right)$$

APROXIMACION DE ALTA TEMPERATURA

$$\rho_{eq}^{HT} = 2^{-N} \left(1 - \frac{\hbar\omega_0}{kT} \sum_i I_{zi} \right)$$

No funciona para campos magnéticos lo suficientemente altos

Warren S. Warren, Science, 262, 2005 (1993)

Solución exacta

$$\rho_{eq} = \sigma_{1,eq} \otimes \sigma_{2,eq} \otimes \cdots \otimes \sigma_{N,eq} \quad \text{Matrices reducidas de espines individuales}$$

$$\sigma_{i,eq} \propto \exp\left(-\frac{\hbar\omega_0}{kT} I_{zi}\right) = \cosh\left(-\frac{\hbar\omega_0}{2kT}\right) 1 - 2 \sinh\left(-\frac{\hbar\omega_0}{2kT}\right) I_{zi}$$

$$\text{Tr}\left[\exp\left(-\frac{\hbar\omega_0}{kT} I_{zi}\right)\right] = 2 \cosh\left(-\frac{\hbar\omega_0}{2kT}\right)$$

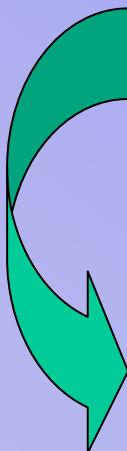
EXACTA

$$\rho_{eq} = 2^{-N} \prod_i (1 - \mathfrak{I} I_{zi}), \quad \text{donde} \quad \mathfrak{I} = 2 \tanh\left(\frac{\hbar\omega_0}{2kT}\right)$$

HT

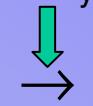
$$\rho_{eq}^{HT} = 2^{-N} \left(1 - \frac{\hbar\omega_0}{kT} \sum_i I_{zi} \right)$$

Coinciden a primer orden



Introduce términos del tipo: $\mathfrak{I}^2 I_{zi} I_{zj}$

90°_y



$$\mathfrak{I}^2 I_{xi} I_{xj}$$

CCD

Evolución con ecuación de Liouville y Hamiltoniano Dipolar

Coherencias cuánticas múltiples

$$\rho(t) = \begin{bmatrix} & |+++ \rangle & |++-\rangle & |+-+\rangle & |+--\rangle & |-++\rangle & |-+-\rangle & |--+\rangle & |---\rangle \\ \langle +++ | & \rho_{11} & \rho_{12} & \rho_{13} & \rho_{14} & \rho_{15} & \rho_{16} & \rho_{17} & \rho_{18} \\ \langle ++- | & \rho_{21} & \rho_{22} & \rho_{23} & \rho_{24} & \rho_{25} & \rho_{26} & \rho_{27} & \rho_{28} \\ \langle +-+ | & \rho_{31} & \rho_{32} & \rho_{33} & \rho_{34} & \rho_{35} & \rho_{36} & \rho_{37} & \rho_{38} \\ \langle +- - | & \rho_{41} & \rho_{42} & \rho_{43} & \rho_{44} & \rho_{45} & \rho_{46} & \rho_{47} & \rho_{48} \\ \langle -++ | & \rho_{51} & \rho_{52} & \rho_{53} & \rho_{54} & \rho_{55} & \rho_{56} & \rho_{57} & \rho_{58} \\ \langle -+- | & \rho_{61} & \rho_{62} & \rho_{63} & \rho_{64} & \rho_{65} & \rho_{66} & \rho_{67} & \rho_{68} \\ \langle --+ | & \rho_{71} & \rho_{72} & \rho_{73} & \rho_{74} & \rho_{75} & \rho_{76} & \rho_{77} & \rho_{78} \\ \langle --- | & \rho_{81} & \rho_{82} & \rho_{83} & \rho_{84} & \rho_{85} & \rho_{86} & \rho_{87} & \rho_{88} \end{bmatrix}$$

± 3 Coherencias cuánticas triples

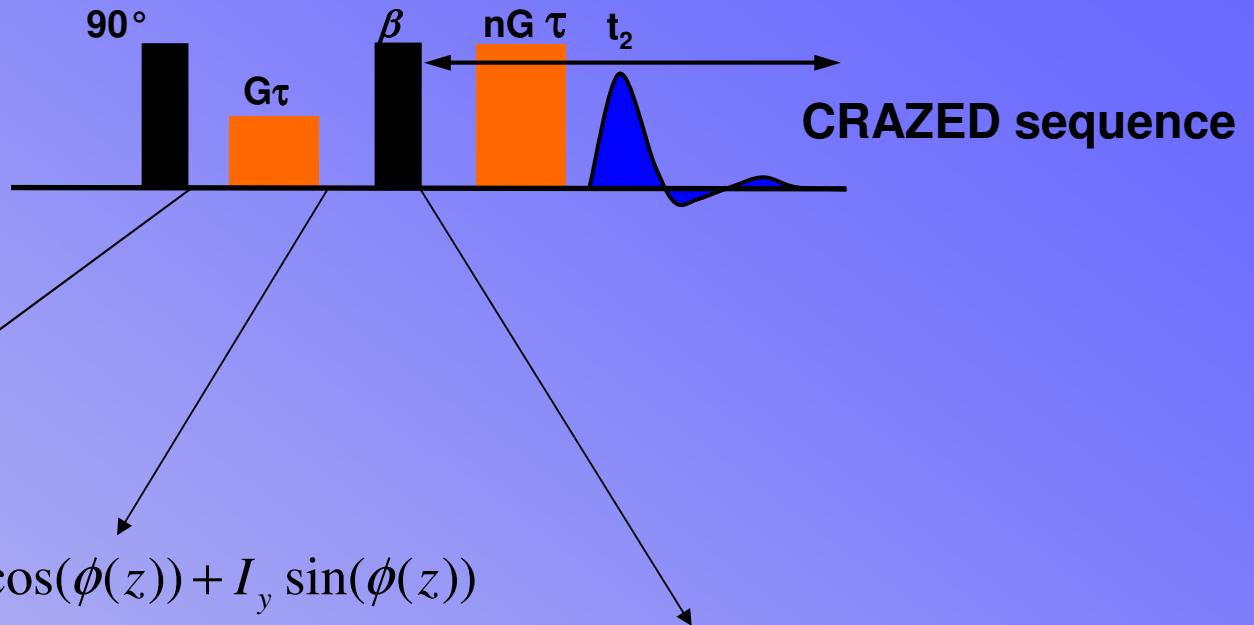
0 Poblaciones

± 1 Observables por RMN

Medición de i-MQC – Marco clásico

Fase introducida por
Gradientes

$$\phi(z) = \gamma G_z \tau$$



$$\rho(\tau^+) = I_x \cos(\phi(z)) \cos \beta - I_z \cos(\phi(z)) \sin \beta + I_y \sin(\phi(z))$$

Dipolar Demagnetizing Field

$$B_d = -\frac{1}{\gamma \tau_d} \cos(\phi(z)) \sin \beta$$

Dipolar Demagnetizing Time

$$\tau_d = \frac{1}{\gamma \mu_0 M_0}$$

CONDICIONES { Magnetizacion alta
Difusion baja

Tarde como siempre ...

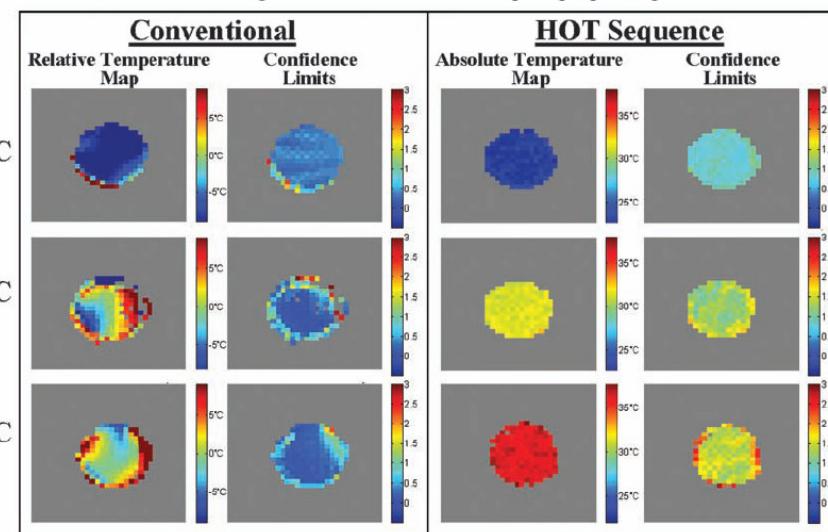
Accurate Temperature Imaging Based on Intermolecular Coherences in Magnetic Resonance

Gigi Galiana,^{1,2} Rosa T. Branca,² Elizabeth R. Jenista,² Warren S. Warren^{2*}

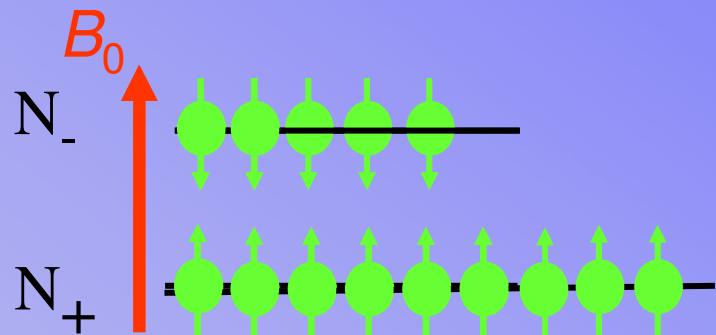
Conventional magnetic resonance methods that provide interior temperature profiles, which find use in clinical applications such as hyperthermic therapy, can develop inaccuracies caused by the inherently inhomogeneous magnetic field within tissues or by probe dynamics, and work poorly in important applications such as fatty tissues.

suitable for imaging temperature in a wide range of resonances of intermolecular zero-quantum coherence flipping down a nearby fat spin. We show that we can measure temperatures *in vivo* on an absolute scale.

Temperature, one of the most fundamental intrinsic quantities of matter, is very difficult to measure noninvasively beneath the surface of an object. A general method to image interior temperatures in soft matter could find a wide range of experimental applications



Sensitividad en RMN



Magnetization: $M_0 = \frac{1}{2} N_s \gamma \hbar P$
($I=1/2$)

Polarization: $P = \frac{N_+ - N_-}{N_+ + N_-}$

Boltzmann: ~~$\frac{N_-}{N_+} = \exp\left(-\frac{\gamma \hbar B_0}{kT}\right)$~~ $\xrightarrow{\gamma \hbar B_0 \ll kT}$

$$P \approx \frac{\gamma \hbar B_0}{2kT}$$

hyperpolarized gases
(^3He , ^{129}Xe):

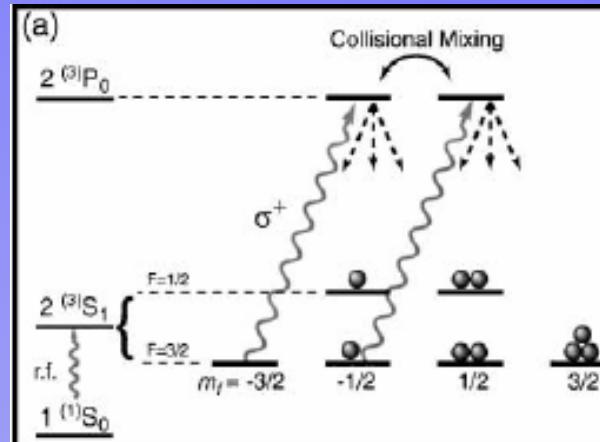
$$P \approx 10^{-1}$$

(factor > 10000)

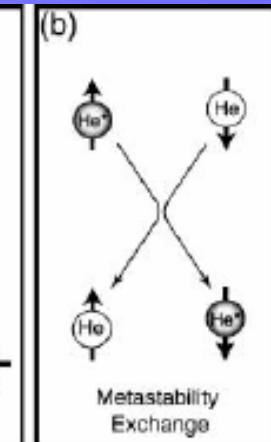
$$P \approx 5 \cdot 10^{-6}$$

Metastable ${}^3\text{He}$ Pumping

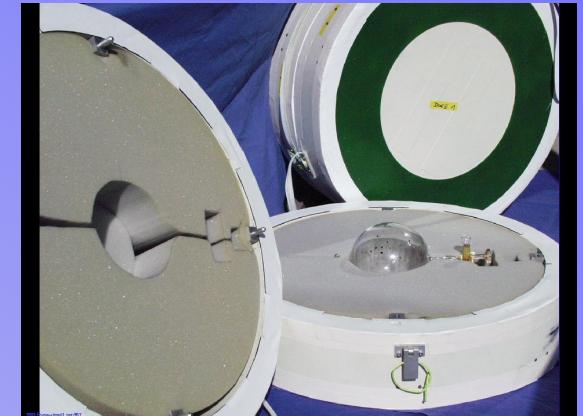
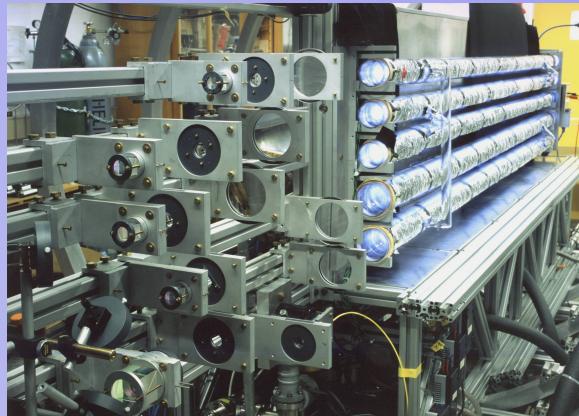
LASER
 $\lambda = 1083\text{nm}$



Electronic Energy levels



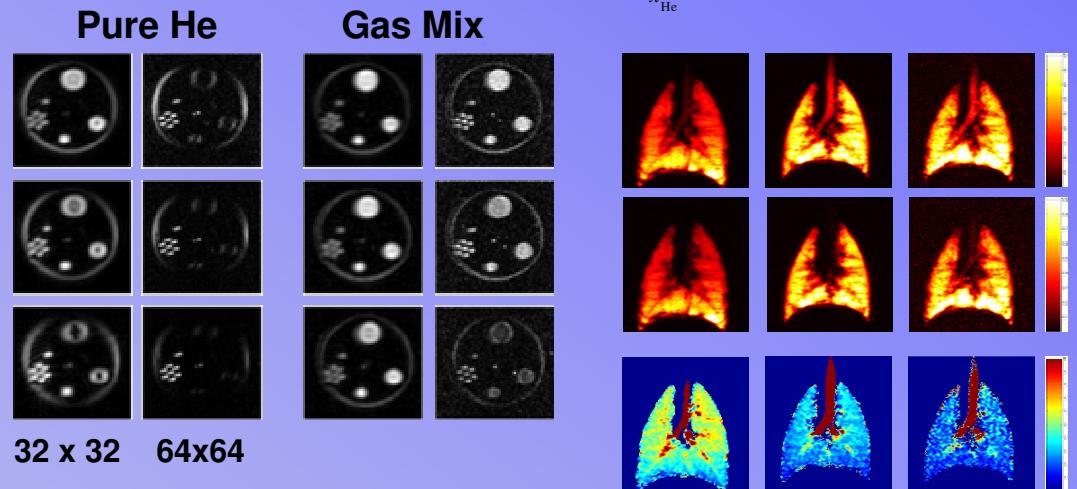
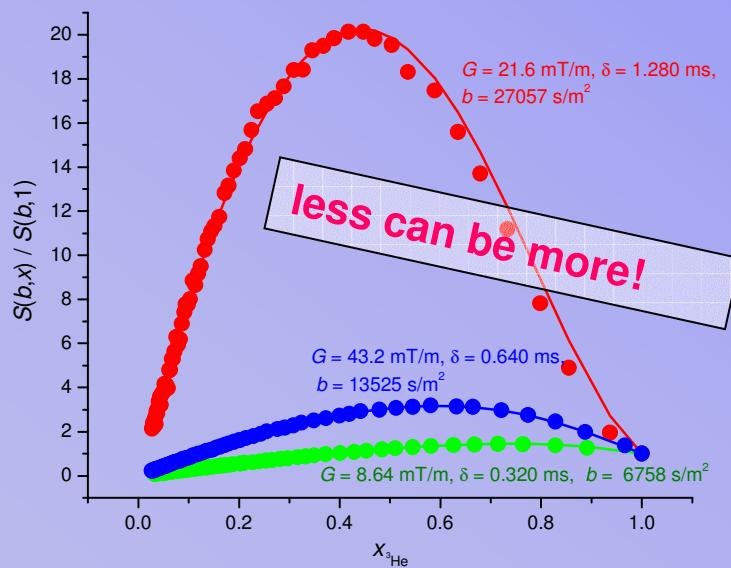
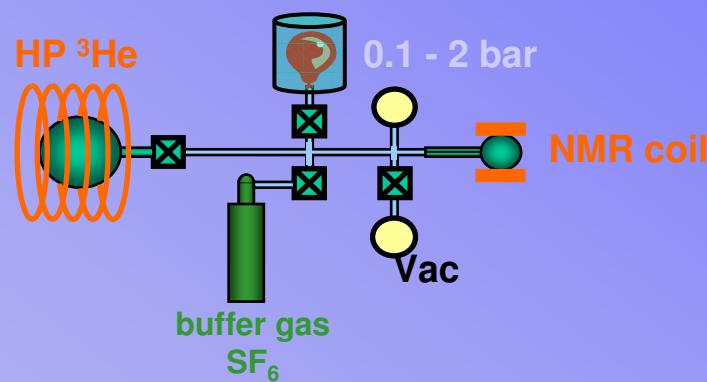
Polarization Transfer



Transport box

Manipulacion del coeficiente de difusión mediante mezcla de gases

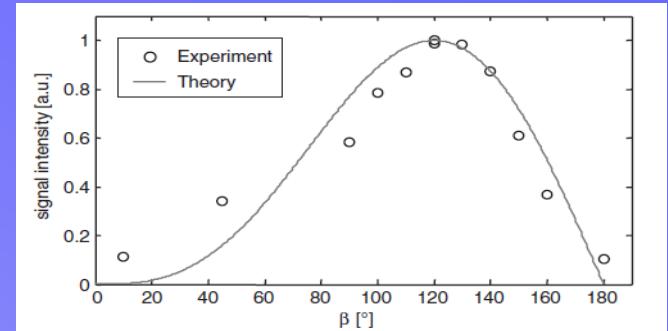
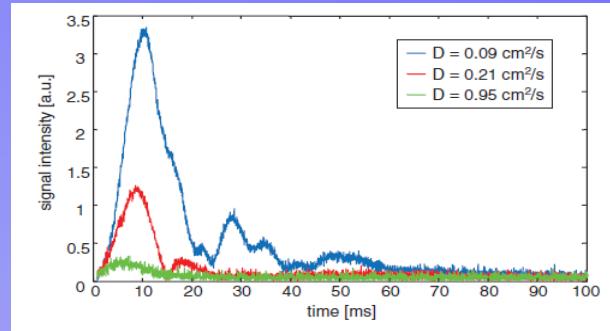
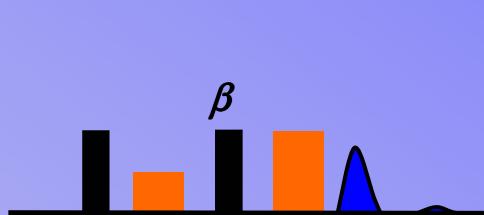
Fully automated – Matlab controlled



Exp. Lung. Research, **30**, 73 (2004)
Magn. Reson. Imag. **22**, 1077 (2004)
JMR. **197** 56 (2009)

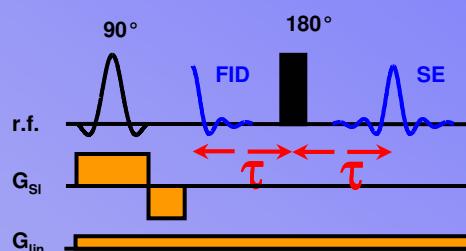
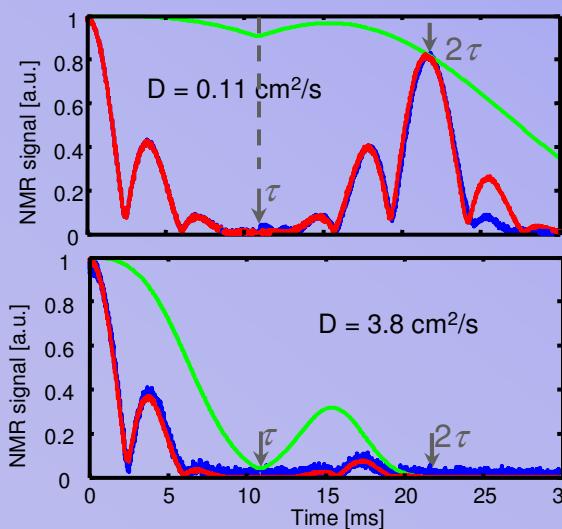
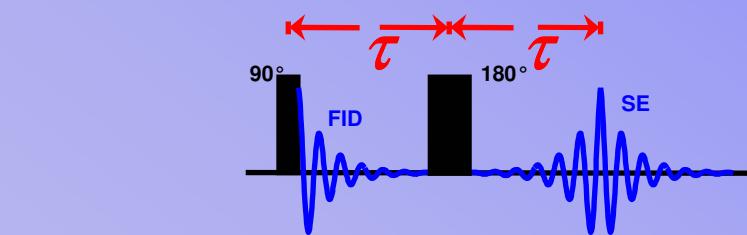
PCCP, **8** 4182 (2006)
JMRI. **24** 1291 (2006)

iDQ in ${}^3\text{He}$ para distintos coeficientes de difusión



PRL 100, 213001 (2008)

Atenuación del eco debido a difusión



Señal nuclear

$E(t) = M(t) \cdot A_{\text{Diff}}(t)$

Atenuacion por difusion

$$A_{\text{Diff}}(2\tau) = \exp[-\frac{1}{2} \gamma^2 G^2 D (2\tau)^3] \quad \text{Formula usual}$$

$$A_{\text{Diff}}(t) = \exp[-\frac{1}{2} \gamma^2 G^2 D (4\tau^3 - 4\tau^2 t + \frac{2}{3} t^3)] \quad , t > \tau$$

$$t_{\max} = \sqrt{2}\tau$$

PRL 99, 263001 (2007)
CPL, aceptado para publicacion

Seminario GTMC - 08/09

Perspectivas

Desarrollar marco teórico para influencia de difusión restringida en i-MQC. Aplicación a nanotubos.

Mapas de difusión del coeficiente de Difusión en pulmones a través de i-DQC.

Detección de señales intermoleculares en parahidrógeno:

$$\rho_{eq} = I_{1z}I_{2z} \quad \rho_{eq} = I_{1z}I_{2z} + \frac{1}{2}(I_{1z} - I_{2z})$$

Transferencia de señales i-MCQ a nucleos raros.